DextrES: Wearable Haptic Feedback for Grasping in VR via a Thin Form-Factor Electrostatic Brake

Ronan Hinchet¹, Velko Vechev ²†, Herbert Shea¹, Otmar Hilliges²
¹EPFL, ²ETH Zurich
{ronan.hinchet, herbert.shea}@epfl.ch, {velko.vechev, otmar.hilliges}@inf.ethz.ch

ABSTRACT
We introduce DextrES, a flexible and wearable haptic glove which integrates both kinesthetic and cutaneous feedback in a thin and light form factor (weight is less than 8g). Our approach is based on an electrostatic clutch generating up to 20 N of holding force on each finger by modulating the electrostatic attraction between flexible elastic metal strips to generate an electrically-controlled friction force. We harness the resulting braking force to rapidly render on-demand kinesthetic feedback. The electrostatic brake is mounted onto the index finger and thumb via modular 3D printed articulated guides which allow the metal strips to glide smoothly. Cutaneous feedback is provided via piezo actuators at the fingertips. We demonstrate that our approach can provide rich haptic feedback under dexterous articulation of the user’s hands and provides effective haptic feedback across a variety of different grasps. A controlled experiment indicates that DextrES improves the grasping precision for different types of virtual objects. Finally, we report on results of a psychophysical study which identifies discrimination thresholds for different levels of holding force.

Figure 1. DextrES is a flexible and thin form-factor haptic feedback mechanism for precise manipulation of virtual objects in VR and AR. a) Our approach provides kinesthetic feedback via electrostatic brakes and piezoelectric actuators for cutaneous feedback. b) We experimentally show that DextrES improves precision of virtual object manipulations in VR across c) a number of different types of grasps, each affording different hand poses.

INTRODUCTION
The dexterity of the human hand enables us to perform a number of useful everyday tasks such as actively exploring surfaces and grasping and moving objects [20, 16]. In Virtual Reality (VR), dexterous manipulation using the hand is a popular means of interaction. It allows us to leverage learned motor skills and vice versa, to train for real-world scenarios in VR [19]. While rapid progress has been made on the input side (display and sensing technologies), haptic interfaces providing physical feedback to the hand lag behind in their fidelity. In particular, the lack of appropriate kinesthetic feedback limit our ability to precisely steer and place grasped objects in 3D space [34].

The ability to grasp objects is amongst the most useful skills we can perform in VR [8]. One challenging aspect is the wide array of possible grasps which require the fingers to be free to move into different configurations [16]. Traditionally, grasping feedback in VR has been supported via glove-based exoskeletons which create braking forces on the fingers [12, 21], render localized tactile feedback on the fingertips [13, 31], or combine aspects of both [10, 22]. These devices often employ complex mechanisms placed around the hand which may either add weight, constrain the movement of the fingers, or both. As a result, the full range of interaction capabilities of the human hand are under-utilized.

To address this challenge, we introduce DextrES, a finger-mounted haptic mechanism capable of achieving up to 20N of holding force on each finger when flexing inward. Our
novel approach is based on electrostatic attraction to create a rapidly controlled braking force between two electrically charged strips of metal. We harness the resulting braking force to rapidly render on-demand kinesthetic feedback which blocks the motion of the fingers. Crucially, this allows for the design of a very thin and flexible form factor haptic interface for grasping objects in VR - a long standing goal which has thus far relied on space-inefficient and bulky mechanisms. Such an interface may also be generalized to function beyond VR, for example in Augmented Reality (AR), robotic tele-operation, and rehabilitation applications.

In contrast to a one-size-fits-all mounting solution, we integrate DextrES onto the index finger and thumb using modular fittings with different strip lengths inserted into 3D printed articulated guides to keep them moving smoothly. The strips are anchored onto the fingertip and wrist resulting in controlled frictional forces due to sliding when the finger is flexed. This mounting strategy allows for easy adaptation to different hand sizes. We couple our kinesthetic brake with miniature vibration motors mounted at each fingertip to signal initial contact events, mimicking a typical object manipulation cycle [24]. The resulting integration into VR allows freedom of movement for both the fingers and hand. The volume of the control electronics can be reduced to a few cm³ with off-the-shelf components, and the very low power consumption (less than 100 mW) allows for battery powered operation, providing a straightforward path to widespread real-world implementation.

We test the capabilities of DextrES in two experiments. First, we establish the just noticeable difference (JND) at different voltage levels and associate this to equivalent holding forces and perceived stiffness values. Second, we explore the impact of our feedback mechanism on the precision of four different grasps (see Figure 1c) in a VR environment. Results indicate that DextrES provides effective feedback and improves precision. Finally, we report qualitative results and user feedback on the perceived user experience when interacting in a free-form VR environment.

RELATED WORK

Haptic Components of Grasping

The perceptual mechanisms behind the experience of holding an object or exploring the shape and texture of its surface is composed of kinesthetic and cutaneous components [23]. Kinesthetic feedback is based on larger scale forces while cutaneous stimuli are felt by the pressure receptors in the skin, typically in the fingertips. During object manipulation, the typical cycle starts when type 1 fast receptors in the fingertips are excited for about 1 second, indicating the contact boundary of an object [24]. After initial contact, kinesthetic forces are transmitted through the joints and muscles, informing us of relative limb and finger positions through the sense of proprioception. Kinesthetic and cutaneous channels work in tandem to provide an accurate sensation of touch [43] that also acts as a feedback loop to accurately control the grasping force exerted on an object [47].

Grasping in Virtual Reality

Researchers have replicated various types of forces in VR which are rendered when grasping an object, including gravity [7, 30], contact [31], shearing [42], rendering hard surfaces [21], and spring-back [8]. While many different types of grasps are possible [16], most grasping devices focus on finger-opposition power grasps. Grounded devices can create high fidelity feedback [29, 1], but are fixed in position. Hand-held VR controllers such as the Oculus Rift and HTC Vive allow the user to move his or her arms freely, but occupy the grasp thus prevent most hand movements, as well as only render coarse vibro-tactile feedback. Our approach consists of a thin form-factor electrostatic brake which can render kinesthetic and cutaneous haptic feedback in a wide range of grasps, affording a rich set of interactive capabilities.

Kinesthetic haptic feedback gloves

Haptic feedback gloves have a long history in HCI and VR research [35]. A number of exoskeletal devices have been proposed to provide kinesthetic haptic feedback by blocking fingers’ movement. We can distinguish between gloves based on pneumatic or hydraulic systems, and those based on electromechanical systems. Gloves based on fluids generally use pumps and valves [22] to displace pistons [17, 5] or activate jamming layers [49, 6] on the glove. These technologies are well-known, but difficult to miniaturize and can result in complex and bulky systems. Gloves using magnetorheological fluids have also been reported [4, 48]. Gloves using electromechanical principles mostly make use of motors or brakes directly on the glove (early versions used very long cables [12]). They use servo motors linked to bars/rods over the top of the hand [28, 27] or cables (tendon-based) across the top of the hand [12, 10, 44] to control finger position. They can actively steer mechanical linkages for finer control. Others have used motors to drive clamp braking mechanisms in order to block the finger [8, 21].

Motors or pumps can offer significant forces, but their performance decreases quickly when scaled down. It is very difficult to maintain sufficient force if scaled to volumes of a few cubic centimeters. Larger motors or pumps may be acceptable for VR but it would be disturbing for AR [35]. It would be ideal to directly be able to lock the finger position without using motors, just by blocking or clutching directly jointless flexible links (cables or strips) connected to the finger. We report here such a solid-state device, a jointless exoskeleton where the only moving parts are actuated by the user.

Electrostatic braking mechanisms

Numerous types of brakes, and more generally clutches, have been developed. Electromagnetic clutches are the most common type of electrically driven clutch, but are bulky and have high power consumption [38]. Mechanical latches can significantly decrease power consumption at the cost of increased complexity and reduced speed. Magnetorheological (MR fluid) clutches are simpler but heavier and consume more energy [46, 40, 45]. Such clutches or brakes are not well suited to haptic gloves for VR and AR applications, where the wearable haptic systems should be as comfortable and discreet as possible.
variety of grasps and enables precise VR manipulations. Kinesthetic and cutaneous feedback and can thus support a rich set of hand poses. Together with piezo actuators, mounted at the base of our glove, we can achieve a high-fidelity haptic feedback mechanism that can be integrated into a VR glove without hindering the natural motion of the fingers. This is crucial for accurate control of frictional and cutaneous feedback, especially in virtual and augmented reality applications.

In contrast, our work explores the use of ES brakes as thin, form-factor electrically driven haptic gloves able to produce kinesthetic feedback. The total weight is less than 8 grams. The ES brake is flexible, allowing for natural hand motion and hence a variety of grasps.

**SYSTEM OVERVIEW**

The aim of our work is to provide haptic feedback for dexterous manipulation of virtual objects in VR and AR. The ideal feedback mechanism would be able to provide both kinesthetic and cutaneous feedback [23] while not encumbering the natural motion of the users' fingers and requiring minimal user instrumentation. This is challenging to achieve since most mechanisms that can provide sufficient force to block finger motion also require significant user instrumentation and are bulky.

Recent work has therefore opted to only support haptic feedback for a limited number of hand poses via actuation mechanisms that are build into a VR controller [3, 9].

In contrast, our work explores the use of an ES brake as thin, form factor kinesthetic feedback mechanism that can be integrated into a VR glove without hindering the natural motion of the fingers. Together with piezo actuators, mounted at the fingertips, DextrES, illustrated in Figure 2, provides both kinesthetic and cutaneous feedback and can thus support a variety of grasps and enables precise VR manipulations.

**Challenges**

While the basic concept of ES brakes is straightforward and has been leveraged for non-haptic applications, designing an effective feedback mechanism for VR is not. To allow for unencumbered motion, the device needs to be thin-form factor and lightweight. Yet to provide effective haptic sensations, it must produce sufficient forces and must be easily mounted on users’ hands of varying sizes. Throughout this paper we discuss our solutions to the following challenges:

1. **Fabricating an ES Brake.** The brake must have sufficient force, speed, be robust, have a low-form factor and sub-Watt power consumption. These requirements impact material and thickness choices for the conductor and insulator layers. Since the brake must conform to the finger shape, the metal strips must be made from a strong and flexible material able to repeatedly bend, yet also provide a small restoring force, thus excluding ductile metals like copper or soft materials like conductive fabrics. The dielectric layer also impacts mechanical and electrostatic aspects and must hence be chosen to be thin enough to attain useful forces without requiring tens of kV, must have a high breakdown field and very low leakage current. Furthermore the dielectric must be flexible and smooth enough to allow accurate control of frictional forces to allow or block the sliding of the strips.

2. **Haptic Glove Integration** The human hand moves in complex ways, typically modeled by a total of 27 degrees-of-freedom [15]. This dexterity poses significant challenges for the design of haptic feedback mechanisms. First, the braking mechanism must be securely mounted onto the users’ hand such that it can effectively brake the motion of fingers in arbitrary poses. To effectively deal with metacarpal abduction (particularly challenging for the thumb) the force needs to be anchored at the back of the hand. Furthermore, to allow for natural motion the brake should not create friction when disengaged. Finally, to accommodate varying hand sizes the mounting mechanism must be flexible and modular.

3. **VR Integration.** Since VR affords a very immediate form of interaction, a haptic feedback mechanism should be able to function efficiently under arbitrary hand poses. In particular, humans use a variety of grasps [16] and as many as possible of these should be supported. To support dexterous object manipulation in VR, the braking mechanism must be able to engage and dis-engage almost instantaneously to allow for rapid, natural hand motion corresponding to a realistic sensation of grasping and releasing virtual objects.

**ELECTROSTATIC BRAKING MECHANISM**

In this section we present the working principle, fabrication process and performance of the electrostatic kinesthetic haptic feedback brakes.

**Operation principle**

At the heart of our approach is a laminar electrostatic (ES) brake. Our ES brake consists of 18 cm long thin flexible metal strips that slide freely when no control voltage is applied, but generate up to 20 N of holding force per pair of strips when a suitable control voltage is applied. One of the key features of the ES brake is its thin form-factor, ideal for
wearable applications. The active part of the brake is conformable to fingers and can be directly mounted or inserted on a glove. The brake mass on the glove is 8 g, and it is 6 mm high (including attachments).

As shown in Figure 1, the ES brake is attached to the glove, covering the back of the hand and the back of the finger. The high degree of flexibility allows excellent conformity to any hand shape. Figure 3 shows the structure of a single ES brake strip (the strips can be stacked to increase force). Each brake element consist of two 100 µm micron thick steel strips, separated by a thin insulation layer bonded to one strip, thus forming a variable capacitor $C_{\text{strip}}$:

$$C_{\text{strip}} = \frac{\varepsilon_r \varepsilon_0 A}{d},$$

where $\varepsilon_r$ is the relative permittivity of the insulator between the electrodes, $\varepsilon_0$ is the permittivity of vacuum, $A$ is the overlap area between the electrodes, and $d$ is the thin dielectric gap between the electrodes. One strip (the “hand strip”) is attached via the glove to a fixed point on the back of the hand, while the other strip (the “finger strip” is attached via the glove to a fingertip. When the voltage difference between the strips is zero, the strips freely slide with a very low friction, enabling full and unimpeded finger movements (Figure 3b). In the simplest model of the device, when a voltage $V$ is applied between the strips, an attractive electrostatic force $F_{\text{compression}}$ is generated between the strips, pulling them together (Figure 3c):

$$F_{\text{compression}} = \frac{\varepsilon_r \varepsilon_0 AV^2}{2d^2},$$

This electrically-controlled normal force leads to frictional forces between the strips, partially or fully blocking the movement of the finger. The friction force is less than or equal to the friction coefficient $\mu$ times $F_{\text{compression}}$:

$$F_{\text{friction}} \leq \mu F_{\text{compression}}.$$  

The higher the applied voltage, the higher the friction force. Using this ES brake, we can thus apply a high blocking force to the fingers, providing kinesthetic haptic feedback.

The power consumption $P_{\text{ESbrake}}$ of the brake is determined by the energy to charge the capacitor multiplied by the switching frequency $f$:

$$P_{\text{ESbrake}} = \frac{E}{t} = \frac{1}{2} CV^2 f$$

Operating at 20Hz and 1.5 kV, the device power consumption is less than 60 mW.

**Fabrication of the ES brake**

After introducing the general working principle we now detail our solutions to challenge Nr. 1 as outlined in the System Overview Section.

We chose stainless steel as conductor since it is a reliable spring material. The bending stiffness of a strip scales approximately with the cube of the shim thickness. One must find a suitable compromise between being thick enough for the shim to slide easily without buckling or plastically deforming, yet thin enough so that the force to bend the strip is nearly imperceptible.

The fabrication of the ES brake strips consists of 3 steps: first, two strips 18 cm long and 1 cm wide were laser cut from 100 µm thick stainless steel sheets. Strips are shortened at a later time to fit the user’s hand and fingers. Using this ES brake, we can thus apply a high blocking force to the fingers, providing kinesthetic haptic feedback.

The power consumption $P_{\text{ESbrake}}$ of the brake is determined by the energy to charge the capacitor multiplied by the switching frequency $f$:
limited the current to 500 µA. Not a problem as long as the current is very small. Hence, we and be firmly attached to it.

The ES Brake must conform as much as possible to the hand (dynamic) across users. To deliver effective haptic feedback, for variations of hand size, geometry (static) and flexibility (wide) and 3D printed guides (6 mm high and 14 mm wide), printed wrist and finger tip anchors (4.5 mm high and 16 mm wide), and the thumb via velcro fabric hook and loop fasteners, 3D printed guides to the thin nylon glove using velcro.

We use 3D printed guides to keep the strips aligned on the edges and covered the strips' free ends with insulating tape. We carefully designed our 3D printed guides to ensure that the multiple degrees of freedom of the thumb, etc. We report here only the configuration that gave the best results.

**Glove assembly**

We mount the ES brakes on a glove covering the index finger and the thumb via velcro fabric hook and loop fasteners, 3D printed wrist and finger tip anchors (4.5 mm high and 16 mm wide) and 3D printed guides (6 mm high and 14 mm wide), see Figure 4. Assembly is straightforward and can account for variations of hand size, geometry (static) and flexibility (dynamic) across users. To deliver effective haptic feedback, the ES Brake must conform as much as possible to the hand and be firmly attached to it.

**Finger flexion and abduction**

The fingers consist of 3 phalanges (2 for the thumb), with joints able to bend up to 90 degrees and with radius of curvature of just a few mm. This range of motion can cause problems when bending a stack of sliding strips. We therefore designed the “hand strip” to be slightly shorter than the “finger strip”. The “finger strip” is attached to the finger tip and covers the phalanges and the metacarpus while the “hand strip” is attached to the wrist and only covers the carpus and metacarpus. The overlap region covers the metacarpus on the back of the hand, anchoring the force so that it can counteract finger flexion.

Another challenge arises from the metacarpo-phalangeal (MCP) joint which can both flex and abduct. If not counteracted, under abduction the free end of the “finger strip” will laterally slide on the back of the hand while rotating the finger, causing misaligned strips and reduced braking force. It is important to maintain a constant distance between the strips, even under deformation. Finally, a misaligned strip can damage the insulating layer. To avoid this, we polished the strips’ edges and covered the strips’ free ends with insulating tape. We use 3D printed guides to keep the strips aligned on the back of the hand, requiring the “finger strip” to be flexible enough to accommodate finger rotation.

**Thumb**

The thumb is composed of only two phalanges and a flexible metacarpus. Designing an ES Brake for the thumb proved to be more difficult than for other fingers. The ES Brake device is the same for all fingers (only its length changes) but its integration on the glove is different for the thumb. We empirically found that to be effective and to support the Power, Pincer, Lateral and Parallel grasps (Figure 1c) we had to tilt the thumb strips anchors 30 degree outward. Moreover, the hand strip had to be attached further back on the wrist compared to the index finger (Figure 1a).

**Glove activation and deactivation**

In the simplest model, the electrostatic force scales as 1/gap², thus having a small initial distance between strips is critical. We carefully designed our 3D printed guides to ensure that a) the strips are as close together as possible, and b) leave just enough room for smooth gliding to allow fast retraction. To activate the brakes, each ES strip is set to 1 kV at 20 Hz. Once a small region of the strip pairs come into contact, the adhesion propagates in a zipper-like effect. To deactivate the brakes, the difference of electrical potential between the strips is set back to 0 V.

**INTEGRATION INTO VR**

**Tracking and Haptic Device Control**

Creating a convincing method of grasping objects in VR requires precise tracking of the fingers in order to determine when contact has been made. For tracking, we use an OptiTrack tracking system with 10 Prime 13 W cameras running at 240 Hz and custom designed rigid bodies that screw into the tips of the fingers. The centroids of the rigid bodies are calibrated to sit in the center of the finger such that finger collisions in real life match finger collisions in VR. The mean
tracking error after calibration of the whole system was < 1
mm. An Oculus CV1 headset is used to display the virtual
scene. The coordinate systems are aligned via a calibration
procedure built into the Motive/Tracker software. We use
Unity to render the VR scenes. The position of the fingers
are displayed as small spheres. Each haptic controller (index,
thumb, piezo) has a separate physical connection (USB) and
are controlled individually over different serial ports.

Grasping Method
We implement a custom grasping algorithm, similar to Choi
et al. [9] using a kinematic approach. A grasp begins when
the position of each finger (index, thumb) are within 5 mm of
a virtual object and the object to be grasped is between the
fingers. Once the object is grasped, the resulting ray between
the two fingers is used to kinematically rotate and re-position
the object in real time, and to calculate the amount of ob-
ject penetration for analysis. The grasp ends when the ray
between the fingers exceeds its original starting (euclidean)
distance. This approach ensures a steady and natural feeling
grip and supports more types of grasps than off-the-shelf so-
lutions such as the Leap Motion Interaction Engine.

Haptic Rendering
When a user grasps an object, we activate index and thumb
brakes simultaneously. Any slack will initially be perceived
as zero blocking force, but as soon as the slack is taken up,
it will be perceived as a sudden locking of the finger. Me-
chanically, the strips counteract torque in the DIP and hence
directly brake the downward motion of the fingertip. The
perceived effect is that of grasping an object in real life, de-
spite not directly generating a normal force. It is possible
that a user could squeeze hard enough to break the adhesion,
however, this would exceed normal grip forces during grasps
which are shown to be two times the load force [47].

In accordance with perceptual theory on initial contact during
object manipulation [24], the feeling of grasping can be im-
proved by adding tactile feedback at the fingertips. For this
task, we use tiny vibration motors (PiezoVibe from Murata)
which measure 3.8 x 10.5 x 2 mm and vibrate at 240 Hz.
They generate an acceleration of 1.2 G for a mass of 20 g and
consume 6 mW. When a grasp begins, we briefly activate the
piezos for 0.3s to indicate the start of a touch event. They are
not re-activated during release.

SYSTEM EVALUATION
Before reporting on our usability experiments we briefly char-
acterize the ES brakes in terms of blocking force vs. applied
temperature and for response speed.

ES Brake predicted force and speed
Based on Equation 2 and Equation 3, and considering an ES
brake having an overlap of $A=11 \, \text{cm}^2$, a $13 \, \mu \text{m}$ Polyimide in-
sulator film with relative dielectric constant 3.4 and a friction
coefficient of 0.2 between kapton and steel [41], a voltage of
1500 V should generate a compression force of 220 N, result-
ing in a friction force of 44 N. Using our HV supply with a
maximum current of 500 $\mu$A, it should take 50 ms to fully
charge the strips, thus enabling up to 20 Hz operation. At this
frequency, the ES brake consumes 57 mW (Equation 4).

Measurement method
To measure the braking force of our ES brake, we placed it in
a pull tester (Instron 3344L) equipped with a 50 N load cell
(Instron 2519). This allows us to pull on the ES brake over
10 mm while measuring the braking force (Figure 5a).

Experimental results
Figure 5b plots the braking force generated by the ES brake
vs. time for a pull speed of 1 mm/s for a 10 Hz AC actuation
voltages ranging from 0 V to 1500 V (Figure 5b). The force
starts at zero and quickly increases as any slack is taken up.
The force then reaches a plateau corresponding to the braking
force. At maximum load, we noted repeated slipping and slip-
stick behavior as a result of the AC actuation.

Results are summarized in (Figure 5c) for 16 measurements
on several devices. Our ES brakes can block up to 20 N at
1500 V and 10 Hz with variations of 10 %. This corresponds
to a force of 2 N/cm². It is possible to stack ES brakes to
achieve higher forces or to reduce the operating voltage at
constant force. When switching between 0 V (free) and 1500
V (locked), we observed a response time of less than 100 ms.
This correspond to a force slew rate higher than 200 N/s.

USER EVALUATION
To better understand the efficacy of DextrES and its possi-
ble applications, we conduct a quantitative and a qualitative
experiment. First, a psychophysical evaluation measures the
just noticeable difference (JND) of stiffness which can be felt
on each finger. Second, we explore the grasping precision
afforded by DextrES and its effect on the immersion of the
user. Each study has been designed to answer the following
research questions respectively:

• RQ1: What is the just noticeable difference of blocking
force at different voltages at each finger (index, thumb) and
what is their associated perceived stiffness?

• RQ2: What effect do the kinesthetic, cutaneous, and com-
bined modes of DextrES have on the precision and immer-
sion while grasping and manipulating objects in VR?

Study 1: Force Discrimination
While grasping devices have been created that can exert up
to 100N of force per finger [8], it is not clear that such high
forces are actually needed for dexterous manipulation of ob-
jects in VR. In this study, we are interested in the perceived
stiffness rendered on each finger (thumb, index) and its JND.
In order to create the feeling of different levels of perceived
stiffnesses, we vary a reference input voltage, and use an
adaptive staircase method [11] to determine the JND at each
reference voltage. Based on pilot studies, we select three re-
ference voltages (200 V, 400 V, 800 V) and a variable step size
with an initial value of $\Delta V$ to 7.5 %. Before the study, we
measured the force output of the strips at each of the refer-
ce voltage and noted this for later analysis (see Fig. 5).

Participants
We recruited six healthy adult unpaid participants ($M=30.8$;
$SD=3.1$; 1 female) from the ETHZ university campus. Par-
ticipants had an average hand span of 21.7 cm ($SD=1.5$)
as measured from the end of the pinky finger to the thumb. Each participant signed an informed consent form prior to the study.

**Procedure and Task**

The braking mechanism was mounted on the index finger and thumb of each participant. Since we only test one finger at a time, the mounting of the 3D printed guides and their velcro holders can be placed in straight lines extending from the tip of both the index finger and thumb, with the thumb configured in the abducted position. Participants are then given some practice time to get accustomed to the device, after which they put on noise-canceling headphones and a blindfold in order to eliminate interference from external visual and auditory senses. The JND for each finger is then determined using the adaptive staircase procedure [11] described above.

Each trial consists of two runs with randomized presentation order. In one run, the fixed reference voltage is activated, and in the other run, the approaching voltage is activated. On each run, the participant flexes their finger inwards until they sense the blocking force. The participant is unaware of which voltage is used. The initial value for the approaching voltage is +25% of the reference value. In the case of 800 V, it was set at -25% of the reference voltage, however positive and negative JND approaches are typically symmetric [19].

After each trial, we ask participants to identify which of the two voltages was perceived to be blocking their finger more. A correct response brings the voltage in the next trial a step size towards the reference voltage, and vice versa [11]. The step size was halved to 3.75% after the first direction reversal in order to get more accuracy after the initial approach. The procedure is repeated until the direction is reversed 3 times and the reversal points are averaged to get the JND of each starting condition. At the end of the procedure, participants answered how stiff they perceived the blocking force to be.

**Results**

Table 1 summarizes the JND for each finger in different positions and reference voltages. The smallest JND for both fingers is in the middle range (400 V), where participants could adequately sense about 5% differences in blocking force. Based on the perceived stiffness at this voltage, it is possible for DextrES to render objects with different levels of deformable stiffness. At the low end (200 V), the JND rises significantly as we approach a perceptibility threshold. At the high end (800 V), participants were considerably more perceptible than expected and perceived stiffness is still not close to maximum, meaning there is still some room to render objects with very hard but still deformable stiffnesses if the voltage is increased even further. Comparing between the middle and high reference, the results are non-linear, which suggests that there is an upper bound on rendering an object of maximum stiffness.

**Study 2: Grasping Precision and Realism in VR**

To answer RQ2, we conduct a VR study measuring both quantitative aspects of precision during object manipulation, and qualitative aspects of realism during the grasping of objects. We use the same definition of grasp as Feix et al. [16] where grasping stipulates that objects are held firmly in the hand (rigid) and not rotated by moving the fingers (static).

**Participants**

Ten healthy adult subjects (M=27.6; SD=4.14; 2 female) were recruited for our study. Two participants had no previous experience with VR and 1 participant was left-handed.
Each participant signed an informed consent form prior to the study.

Procedure
The procedure is described to the participant alongside a brief introduction to the device and its function. The ES brake strips are then mounted to the back of the hand and adjusted as described earlier. Participants could sit in a 1x1 meter tracking area wearing an Oculus headset. Participants wore noise-canceling headphones to remove external audio cues when grasping objects. The experiment consisted of two scenarios, the first evaluating the quantitative aspect measuring grasping precision, the second, qualitative aspects comparing the realism of grasping objects between different haptic feedback conditions. The experiment took 1.5 hours to complete.

Participants could practice freely in order to learn four different grasps (Lateral, Parallel, Pincer, Power) and to get used to the different types of feedback. After training, 4 blocks were completed of 16 unique grasp/condition combinations for 64 trials in total. The quantitative part was followed by approximately 1 min of each condition in a physics playground which was designed to resemble a typical desk with various sized items which could be grasped and interacted with. The experiment concluded by participants indicating their subjective preferences and a short interview on the overall impression of the experience in using DextrES. We also recorded suggestions for possible applications of our device and informal comments.

Design
For the quantitative study, a within-subject design was used with two independent variables: Grasp {Lateral, Parallel, Pincer, Power} and Feedback {Visual, Piezo, Brake, Both}. The order of each stimuli was randomized such that each combination of Grasp and Feedback was presented once per block. As dependent variables, we measured time and precision for each trial. Precision was measured by the percentage of finger-object penetration averaged over the whole trial.

At the end of the physics playground scenario, we asked participants to rate how realistic the sensation of holding an object is in each feedback condition on a 7-point Likert-scale (1: Extremely unrealistic, 7: Extremely realistic). We also ask about the comfort of the device while turned off (1: Very uncomfortable, 7: Very comfortable) and the freedom of movement (1: Fully blocking, 7: Full range of motion).

Task, Stimuli and Apparatus
Trials were initialized and terminated via pressing a virtual button, or after a 20 second timeout. Each Grasp has an associated task (see Fig. 6 for visuals and explanation) which is derived from real-life tasks. Participants were instructed to complete the task in timely manner as accurately as possible. The instructions given in regards to grasping an object were to perform it as naturally as possible. After each block participants could take a break before proceeding.

Quantitative Results
To assess the effect of the different feedback mechanisms on grasp precision we ran a repeated measures ANOVA for each grasp. There was no difference in terms of task completion times. Since the four grasps are significantly different it does not make sense to compare feedback mechanisms across the four grasps. We now report main effects and pairwise post-hoc comparisons for all four grasps (lateral, parallel, pincer, power) respectively. The sphericity assumption was not violated for any of the grasps. All p-values of pairwise comparisons are Bonferroni corrected.

For the lateral condition (e.g., turning a key) a main effect for the feedback mechanism ($F_{3,27} = 5.17, p < 0.01$) was detected. A post-hoc analysis reveals that both is significantly more precise than brake ($p = 0.02$) but differences to other conditions are not statistically significant.

The parallel grasp (e.g., lifting a book) yields similar results. The analysis again shows a main effect ($F_{3,27} = 4.86, p <
and also helped to identify when grasping an object begins “It helped me understand when I should stop applying force”. The brake-only condition was slightly less preferred due to missing collision information “When you go and touch something you expect your skin to be bump into it”. When the brake was missing, participants could sense its absence “As soon as you go to the next trial and it’s off, you then you miss the feedback”. Two participants preferred the piezo over the brake on its own, however, it was still rated as less realistic as just the brake (e.g. “Its very useful to know when you touch it, but its not a realistic feeling”). Furthermore, the brake adds realism in the context of limiting range of motion (e.g. “If you hold a bigger object, then if you rotate you should have more limited range of motion”) (because the forearm muscles engage). Some participants found DextrES to provide physical support, specifically in the lateral grasp “When I got tired, I was using the brake to rest my thumb”). The main issue w.r.t. to comfort was the feeling of velcro on the hand, but on the whole, participants felt that DextrES was comfortable to wear. In terms of applications, participants wanted to use the device to play games, for virtual typing, and also for creative tools such as CAD tools and painting (e.g. “You can 3D paint, but maybe different sized brushes have different weight”).

DISCUSSION

A major contribution of our work is to fabricate an ES brake for VR. Through careful material selection, specifically the use of a conductive adhesive to minimize effective dielectric thickness and a dielectric with high breakdown fields, in combination with a flexible mechanical design that allows for dimension tailoring and achieves reliable sliding over curled fingers, and by using AC switching of the 1.5 kV power supply to avoid charge injection, we were able to develop an ES brake with suitable force generation capabilities while allowing natural hand motion. Including mounting hardware, DextrES weighs under 8 g. yet can block 20 N when on, with only a few mN of residual force when off. We thus have a blocking force density over 2500 N/kg, while delivering a device so flexible it is barely perceivable on the hand. The materials are all readily commercially available, and can be machined in minutes with a laser cutter.

The ES brake was integrated into a glove using close-fitting 3D printed attachments on the fingertips and wrist, by precise positioning of 3D printed guides on the glove, by aligning the index brake with the index’s long extensor tendon, and by placing most of the active part of the brake on the back of the

Figure 7. Effect of feedback mechanism on precision of 4 grasp types. Conditions are both (red), brake (blue), piezo (yellow) and visual (green). The black dot is the average, the black line is the median, the box corresponds to the IRQ and the bars to the min-max. Lower is better.

Figure 8. Subjective feedback on 7-point Likert scale. Dot is the mean and bars indicate confidence interval. Higher is better.

0.01) and post-hoc analysis reveals that there is a significant difference between both and brake ($p=0.04$), albeit inspecting the plot in (Figure 7) shows that the differences are very small and this result should be interpreted carefully.

The remaining two grasps show a more marked effect of the feedback mechanism on the precision of the grasp, perhaps because both pincer and power admit much more finger motion (cf. Discussion section). There is a main effect for pincer ($F_{3,27} = 12.24, p < 0.01$) and pairwise comparisons indicate that both is significantly more precise than brake ($p=0.01$), piezo ($p=0.02$), and visual ($p < 0.01$). Finally, the power grasp also yields a main effect ($F_{3,27} = 21.32, p < 0.01$). The pairwise comparisons indicate that for this grasp brake is the most precise. However, compared with both ($p > 0.05$) the difference is not statistically significant. Both (brake, both) feedback mechanisms are however statistically more significant than the (piezo, visual) baselines (both vs piezo: ($p=0.01$), both vs visual: ($p < 0.01$)).

Qualitative Results

Subjective Rankings

The physics playground gave participants a chance to interact freely with virtual objects. In terms of the realism (see Figure 8) of the sensation of holding an object participants consistently rated the both feedback condition the highest ($M=5.3; SD=0.5$), followed by the brake ($M=4.4; SD=0.8$) and piezo ($M=3.5; SD=1.1$), and finally the visual only feedback ($M=2.2; SD=0.8$). Participants rated the device as mounted on the hand as fairly comfortable ($M=5.1; SD=1.4$), and the freedom of movement as neutral in terms of limiting finger motion ($M=4.6; SD=0.8$).

Participant Comments

Participants strongly favored the combined feedback, which produced the highest sense of VR immersion (e.g., “Haptic is missing from VR, and I’m really impressed that it can block.” and “It’s pretty cool. It adds a lot of immersion.”),
hand where there is much less deformation. The thumb was most challenging, principally due to its more complex motion (not only can it flex like the fingers, but it can also pivot on 2 axes), making it harder to mount the ES brake in a way that effectively blocks flexion. There is also little room on the back of the hand to mount the brake and a medium curvature close to the wrist attachment. We found that aligning the thumb ES Brake 30 degrees outward of the thumb flexion axis gave the most blocking. While more direct forms of tactile feedback are available [36, 3], integrating such devices in their current form may interfere with the mounting of the strips and the natural motion of the hand.

The final challenge of VR integration was also met. The results from our VR grasping study indicate that DextrES is able to support three of the four grasps (Parallel, Pincer, Power), in particular when both the brake and piezo work in tandem. Participants were able to both pick up and drop objects in a natural fashion and experience a sensation of holding an object. The main differentiating factor between grasps is the distance between the tip of the index finger and the thumb. In the Power grasp, this distance is wide, and thus gives some space for the brake to engage and to exhaust any mechanical slack. As a result, the brake and both conditions perform similarly. In the Pincer and Parallel grasps, this distance is small, thus they greatly benefit from the additional collision signal from the Piezo. With regards to the Lateral grasp, this distance is also small. Furthermore, the inward flexion of the thumb does not necessarily induce any sliding motion on the strips of the brake, and thus neither the piezo or the brake have much stopping effect. While the brake cannot constrain certain degrees of freedom of the thumb in the Lateral grasp, participants enjoyed that they could rest their thumb after the brake has engaged.

The above results show that DextrES is able to increase precision during specific VR manipulations. In same cases and for some participants the differences were small in the controlled experiment. However, in the more natural setting of the physics playground, participants exhibited very different behavior. They were less careful when picking up and handling objects and thus tended to penetrate through them completely in the visual and piezo conditions (see Figure 9, left), whereas with haptic feedback they conformed to the object’s shape (see Figure 9, right). In part, this explains the large differences in the perceived realism in holding an object compared to the smaller differences we see when looking at the percentage of penetration in the controlled experiment. While we do not directly test grasping objects of variable stiffness in VR, results from the force discrimination study suggests that this is a possibility.

CONCLUSIONS AND FUTURE WORK

We have presented DextrES, a novel haptic glove integrating electrostatic braking using flexible components. With its low mass (under 8 g) and high force (over 20 N) it overcomes limitations of more traditional motors and pumps. Our experimental results indicate that DextrES is a very promising step towards soft, flexible, high-speed wearable haptics conveying the sense of grasping with high realism. We tested the device for 4 grasps and found improved grasping precision for different virtual objects. By including small piezoactuators at the fingertips, we further increased the grasping precision.

Naturally, there is much room for future work. We plan to reduce the operating voltage by an order of magnitude by printing thinner dielectric layers or layers with higher permittivity. Lower voltage operation will: i) make the control electronics more compact and much cheaper since all components can be sourced in surface mount format (SMD), ii) reassure users who may be concerned about high voltages, iii) ease regulatory processes for wearables. Users currently are aware of the 20Hz switching, which can be distracting. Lower voltage operation would allow the device to be run with a sine wave rather than a square wave, greatly reducing the audible vibration. Further, the force generation capabilities may be increased by stacking several ES brakes.

In terms of haptics, it will be interesting to produce a five fingered version of DextrES and to study it in more fully fledged VR and AR scenarios, and to explore the interplay between cutaneous and kinesthetic feedback in different manipulation tasks. To free up the fingertips in AR, the piezos could be moved to the side of the fingers and contact forces transmitted through the vibration of curved metal plates.

Finally, we note that it may be possible to reconstruct the hand pose via measuring the change in capacitance of the overlapping metal strips in combination with an inverse kinematics model of the human hand, removing the need for external tracking.

As wearables and VR become more mainstream, richer unobtrusive wearable haptic feedback becomes increasingly important. Lightweight and very low-profile gloves such as DextrES will allow users to benefit from rich and high-force haptics without excessive user instrumentation.

ACKNOWLEDGEMENTS

This work was supported in part by a grant from the Hasler Foundation (Switzerland). We thank Simon Perrault for his help in the statistical analysis, Saham Ayvaz for his contribution in the mechanical design, Alexandru Dancu for experiment design feedback, Lilia Leung for illustration work,

Figure 9. Examples of differences in grasps across conditions. Left: without haptic feedback, participants penetrate virtual objects. Right: with haptic feedback, fingers conform to the object’s shape (green book).
Nadine Besse for mounting the piezo-actuators, Sam Schlatter for electronics advice, Juan Zarate for helpful discussions, and all participants for taking part in our experiments.

REFERENCES


